

Contralateral fatigue during severe-intensity single-leg exercise: influence of acute acetaminophen ingestion

Original investigation

Paul T. Morgan¹, Stephen J. Bailey^{1,3}, Rhys A. Banks¹, Jonathan Fulford², Anni Vanhatalo¹, and Andrew M. Jones¹

¹ Department of Sport and Health Sciences, College of Life and Environmental Sciences, University of Exeter, St. Luke's Campus, Heavitree Road, Exeter, EX1 2LU, UK.

²Peninsula NIHR Clinical Research Facility, College of Medicine and Health, Exeter, UK.

Address for Correspondence:

Professor Andrew Jones

Department of Sport and Health Sciences, College of Life and Environmental Sciences, University of Exeter, St. Luke's Campus, Heavitree Road, Exeter, EX1 2LU, UK.

Tel: 01392 722 886

E-mail: A.M.Jones@exeter.ac.uk

³**Present address for Stephen J. Bailey:** School of Sport, Exercise and Health Sciences, Loughborough University, Epinal Way, Loughborough, Leicestershire LE11 3TU

Running title: Effect of acetaminophen on contralateral leg fatigue

Disclosure of funding: This research was not sponsored by any funding body external to University of Exeter

ABSTRACT

Exhaustive single-leg exercise has been suggested to reduce time to task failure (T_{lim}) during subsequent exercise in the contralateral leg by exacerbating central fatigue development. We investigated the influence of acetaminophen (ACT), an analgesic which may blunt central fatigue development, on T_{lim} during single-leg exercise completed both with, and without, prior fatiguing exercise of the contralateral leg. Fourteen recreationally-active men performed single-leg, severe-intensity knee extensor exercise to T_{lim} on the left (Leg_1) and right (Leg_2) legs without prior contralateral fatigue, and on Leg_2 immediately following Leg_1 ($Leg_{2-CONTRA}$). The tests were completed following ingestion of 1 g ACT or maltodextrin (placebo) capsules. Intramuscular phosphorous-containing metabolites and substrates, and muscle activation, were assessed using ^{31}P -MRS and electromyography, respectively. T_{lim} was not different between the Leg_{1ACT} and Leg_{1PL} conditions (402 ± 101 vs. 390 ± 106 s; $P>0.05$). There was also no difference in T_{lim} between $Leg_{2ACT-CONTRA}$ and $Leg_{2PL-CONTRA}$ (324 ± 85 vs. 311 ± 92 s; $P>0.05$), but T_{lim} was shorter in these tests compared to Leg_{2CON} (385 ± 104 s; $P<0.05$). There were no differences in intramuscular phosphorous-containing metabolites and substrates, or muscle activation, between the Leg_{1ACT} and Leg_{1PL} or the $Leg_{2ACT-CONTRA}$ and $Leg_{2PL-CONTRA}$ conditions ($P>0.05$). These findings suggest that task failure during single-leg severe-intensity knee extensor exercise is associated with the attainment of a similar level of metabolic perturbation and muscle activation, both with and without prior fatiguing exercise of the contralateral leg. Despite the existence of contralateral fatigue, ACT ingestion did not alter neuromuscular responses or exercise performance.

Key words: ^{31}P -magnetic resonance spectroscopy; intramuscular metabolites; intramuscular substrates; non-local muscle fatigue, paracetamol

INTRODUCTION

The mechanisms of exercise-induced fatigue can be attributed to processes within the central nervous system, termed central fatigue, and within the contractile elements of the working muscle, termed peripheral fatigue. It is now recognised that peripheral and central fatigue development are interlinked, in part, via group III/IV muscle afferent feedback (25). Empirical support for a role of group III/IV muscle afferent feedback in modulating the mechanisms of neuromuscular fatigue is provided by reports that inhibiting group III/IV muscle afferent feedback, via lumbar intrathecal administration of fentanyl, lowers central fatigue development and results in increased skeletal muscle metabolic perturbation [greater and/or more rapid increases in adenosine diphosphate (ADP) and inorganic phosphate (Pi) accumulation and declines in phosphocreatine (PCr) and pH] and thus peripheral fatigue development (i.e., 1, 2, 8, 10, 11, 12, 38, 39, 40). Conversely, prior fatiguing single-limb exercise has been reported to accentuate central fatigue development and lead to lower peripheral fatigue development during subsequent fatiguing exercise in a contralateral or non-local (previously rested) muscle group, when group III/IV muscle afferent feedback would be expected to be elevated (3, 22, 23, 26, 33, 40). However, the underlying mechanisms of non-local muscle fatigue, including the effect of prior fatiguing single-limb exercise on skeletal muscle metabolic perturbation during subsequent fatiguing exercise in a contralateral or non-local muscle group, have yet to be resolved (ref. 23 *for review*). Moreover, while lumbar intrathecal administration of fentanyl and prior fatigue of a contralateral or non-local muscle group can alter group III/IV muscle afferent feedback and the physiological bases of exercise-induced neuromuscular fatigue, the effect of such interventions on exercise performance is equivocal (i.e., 1, 2, 3, 8, 10, 11, 12, 22, 23, 26, 28, 33).

There is an emerging body of evidence to suggest that oral ingestion of acetaminophen (ACT) can blunt the development of exercise-induced neuromuscular fatigue and improve exercise capacity and/or performance (19, 30, 31, 32). It is generally accepted that the principal mechanism of action of ACT is the inhibition of cyclooxygenase, the enzyme that catalyses the synthesis of prostaglandins from arachidonic acid (4). Since prostaglandins sensitize nociceptors (36, 37), and since blocking cyclooxygenase attenuates group III/IV muscle afferent discharge during dynamic exercise (24), this might account for reports of increased work output for the same level of perceived pain and exertion (19, 30), and elevated muscle activation (31, 32), during exercise after ACT ingestion. Therefore, ACT administration might be ergogenic by reducing, but not abolishing, the net magnitude of group III/IV muscle afferent feedback, leading to a blunting of exercise-induced central fatigue. Since ACT appears to attenuate exercise-induced neuromuscular fatigue by abating aspects of central fatigue development (19, 30, 31, 32), ACT might be more effective at lowering exercise-induced neuromuscular fatigue following prior exhaustive exercise in a contralateral limb. However, the effects of ACT ingestion on exercise-induced fatigue development and its underlying mechanisms following prior exercise in a contralateral limb have yet to be investigated.

The purpose of this study was to investigate the effects of ACT ingestion on exercise-induced neuromuscular fatigue and some of its underlying mechanisms during single-leg severe-intensity knee extensor exercise completed with and without prior exhaustive severe-intensity knee extensor exercise in the contralateral leg. It was hypothesised that: 1) prior exhaustive exercise would impair subsequent exercise tolerance in the contralateral leg by lowering muscle activation and the degree of muscle metabolic perturbation [changes in muscle pH and PCr ([PCr]), ADP ([ADP]) and Pi ([Pi]) concentrations] that could be attained; 2) ACT ingestion would enhance single-leg knee extensor exercise tolerance by increasing muscle

activation (higher surface EMG) and permitting the attainment of a greater degree of muscle metabolic perturbation; and 3) ACT ingestion would improve exercise tolerance to a greater extent with, compared to without, the completion of prior exercise by the contralateral leg.

MATERIALS AND METHODS

Subjects

Fourteen active males volunteered to participate in this study (mean \pm SD: age 23.8 ± 4.7 y, height 1.80 ± 0.10 m, body mass 81.6 ± 14.9 kg). All procedures were approved by the Ethics Committee of the Department of Sport and Health Sciences, University of Exeter. This study conformed to the principles of the World Medical Association Declaration of Helsinki. Subjects completed a health questionnaire, which was checked by a medical doctor, to ensure it was safe to consume ACT prior to performing exhaustive exercise. The questionnaire incorporated questions pertaining to: known allergies to medications, current intake of medication and prior use of ACT as well as any history of illnesses, cigarette and illegal drug use, alcohol consumption, and chronic illnesses (personal and family history). Prior to each visit, subjects were required to refrain from caffeine (for at least 12 h), strenuous exercise and alcohol (for at least 24 h), analgesics and any form of anti-inflammatory drug (for the duration of the experiment) and to arrive in a fully rested, hydrated state. With the exception of these restrictions, subjects were instructed to maintain their usual diet and exercise regime during the study. All tests were performed at a similar time of day (± 2 h).

Pre-experimental procedures

Subjects visited the laboratory on twelve occasions over an 8-12 week period to complete the experimental testing, with a minimum of 72 h separating all tests (figure 1). The experimental testing incorporated 4 pre-experimental trials (visits 1-4) and 8 experimental trials (visits 5-

12). *Visits 1-4* were completed within a replica of an MRI scanner (with no magnetic field present). Initially, subjects completed a single-limb incremental test on the left leg (*visit 1*, Leg₁) and right leg (*visit 2*, Leg₂) to task failure to establish the limb-specific work rates that would be applied in subsequent experimental visits (as described below). Following these preliminary tests, subjects completed a familiarisation session on *visits 3 and 4* which comprised a single-leg severe-intensity constant work rate (CWR) test to task failure with the left leg (Leg₁), a single-leg severe-intensity CWR test to task failure with the right leg (Leg₂), and a crossover test where the Leg₁ protocol was repeated and immediately followed by the Leg₂ protocol to assess contralateral fatigue in Leg₂. In these preliminary tests, the Leg₁, Leg₂ and Leg₂ contralateral protocols were interspersed by 10 min of passive recovery.

Experimental procedures

During *visits 5 and 6*, subjects completed the Leg₁ and Leg₂ protocols without oral consumption of any capsules (Leg₁CON and Leg₂CON, respectively). On *visits 7 and 8*, subjects completed the crossover limb tests described above, 45 mins following the consumption of 1 g maltodextrin (placebo, PL) to determine time to task failure (T_{lim}) values for Leg₁ (Leg₁PL) and Leg₂ contralateral (Leg₂PL-CONTRA), and 45 mins following the consumption of 1 g ACT, to determine T_{lim} values for Leg₁ (Leg₁ACT) and Leg₂ contralateral (Leg₂ACT-CONTRA). PL and ACT were administered in the form of 2 identically coloured pills. The placebo was made from maltodextrin powder inserted into gelatine capsules designed to have a similar appearance to ACT without inducing any analgesic or antipyretic effects. The oral consumption of PL and ACT ~45 min prior to commencing exercise was selected to broadly coincide with attainment of the peak plasma [ACT], which occurs ~60 min post ACT ingestion (4, 17), at the onset of the Leg₂-CONTRA tests. The PL and ACT conditions were administered double-blind in a counterbalanced cross-over experimental design. *Visits 5-8* were completed within the bore of

an MRI scanner for assessment of exercise-induced changes in intramuscular phosphorous-containing substrates and metabolites. *Visits 5-8* were replicated in *visits 9-12* within a replica of the MRI scanner (with no magnetic field present) to assess muscle electromyography (EMG) and ratings of perceived exertion (RPE).

Experimental set-up

Exercise tests were performed in a prone position within the bore of a 1.5 T superconducting magnet (Gyrosan Clinical Intera, Philips, The Netherlands) using a custom-built ergometer for the assessment of intra-muscular [PCr], [Pi], [ADP] and pH (*visits 5-8*) or within a replica of the MRI scanner for preliminary testing (*visits 1-4*) and the assessment of EMG and RPE responses (*visits 9-12*). Subjects' feet were fastened securely to padded foot braces using Velcro straps and connected to the ergometer load baskets via a rope and pulley system. The sprocket arrangement was such that when a bucket containing non-magnetic weights was attached, it provided a concentric-only resistive load, allowing for the performance of rhythmic knee-extension exercise. Single-leg knee-extensions over a distance of ~ 0.22 m were performed continuously at a constant frequency which was set in unison with the magnetic pulse sequence ($40 \text{ pulses min}^{-1}$) to ensure the quadriceps muscle was in the same phase of contraction during each magnetic resonance pulse acquisition. To prevent displacement of the quadriceps relative to the magnetic resonance spectroscopy (MRS) coil, Velcro straps were also fastened over the subject's thighs, hips and lower back.

Experimental protocol

To determine peak work rate (WR_{peak}) for each leg, subjects initially completed single-leg incremental knee-extensor exercise on *visits 1 and 2* until they were unable to continue the prescribed work rate, as described previously (43). The load for the initial increment was 4 kg

and this was increased by $0.5 \text{ kg} \cdot \text{min}^{-1}$ thereafter until T_{lim} . T_{lim} was recorded when subjects were unable to sustain the required contraction frequency for 3 consecutive repetitions. Following these initial tests, subjects were familiarized with the different exercise tests that comprised the experimental testing protocol. During these visits, a limb-specific, high-intensity work rate, which was expected to elicit T_{lim} in approximately 5–8 min, was prescribed for each subject.

The experimental exercise protocol consisted of CWR, single-leg knee-extension to T_{lim} . Initially, subjects completed single-leg knee-extension exercise for each limb individually over two separate laboratory visits. Subsequently, to investigate the influence of ACT on contralateral leg fatigue, subjects completed single-leg knee-extension exercise until task failure with Leg₁, followed consecutively (<3 s) by the identical task with the contralateral leg (i.e., Leg₂). These crossover tests to assess contralateral fatigue in Leg₂ were completed 60 min following the consumption of PL and ACT over two separate laboratory visits. For all trials, subjects received strong verbal encouragement to continue for as long as possible but no feedback was given on the elapsed time.

MRS measurements

³¹P-MRS data were acquired every 1.5 s with a spectral width of 1,500 Hz and 1,000 data points. Phase cycling with four phase cycles was used, leading to a spectrum being acquired every 6 s. The subsequent spectra were quantified by peak fitting, using the AMARES fitting algorithm in the jMRUI (v3) software package. Absolute values of [PCr] and [Pi] concentrations were subsequently calculated via the ratio of PCr:adenosine triphosphate (ATP) and Pi:ATP assuming an ATP concentration of 8.2 mM. Intracellular pH was calculated using the chemical shift of the Pi spectra relative to the PCr peak. The ADP concentration was

calculated as described by Kemp *et al.* (27). In all cases, relative amplitudes were corrected for partial saturation resulting from the short repetition time relative to T1 relaxation time, via a spectrum consisting of 24 averages that was acquired with a TR of 20 s prior to the commencement of exercise testing.

Electromyography

Throughout *visits 9-12*, muscle activity of the right and left *m.vastus lateralis* was recorded using active bipolar bar electrodes with a single differential configuration (DE2.1, DelSys Inc, Boston, MA, USA). Initially, the leg was shaved and cleaned with alcohol to minimize skin impedance. The electrodes were placed over the respective muscle bellies parallel to the longitudinal axis of each muscle (SENIAM guidelines). Double-sided adhesive tape and a hypoallergenic medical tape were used to ensure the EMG sensor stability. The position of the EMG electrodes was measured with respect to the location of the patella and the anterior superior iliac spine and marked with indelible ink to ensure placement in the same location on subsequent visits. The ground electrode was placed over the patella of the respective leg. The EMG signals were pre-amplified (1,000x), band-pass filtered (20–450 Hz, Bagnoli-8, DelSys Inc, Boston, MA, USA), and then transferred to a computer with a sampling frequency of 2 kHz. EMG data were recorded continuously and digitised synchronously with 16 bit resolution via an A/D converter (± 5 V range, CED 1401 power, Cambridge, UK) using Spike2 software (CED, Cambridge, UK). During these trials, ratings of perceived exertion (RPE) was measured at 2-min intervals from the onset of exercise using Borg's 6-20 scale (9).

Data Analysis

Baseline values for [PCr], [Pi], [ADP], and pH were defined as the mean values measured over the final 60 s of rest (i.e., prior to initiation of the severe-intensity exercise bout). Baseline

values for Leg₂ during the crossover protocol (for both PL and ACT) were calculated during the final 60 s of exhaustive Leg₁ exercise. End-exercise values for these variables were defined as the mean values measured over the final 30 s of exercise. The changes (Δ) in [PCr], [Pi], [ADP] and pH across the protocol were then calculated as the difference between end-exercise and baseline values. [PCr], [Pi] and [ADP] were expressed as absolute concentrations and as a percentage change relative to resting baseline (i.e., 100%). The overall rate of change for [PCr], [Pi], [ADP] and pH was calculated as the difference between end-exercise and baseline values divided by T_{lim}. EMG was average rectified and normalised to the first 30 s of each trial (aEMG). For analysis, T_{lim} values obtained from visits 5-8 were used. Visits 9-12 were used to overlay EMG and RPE responses to ³¹P-MRS data.

Statistics

Differences in T_{lim}, baseline and end-exercise aEMG and muscle [PCr], [Pi], [ADP], and pH between control limbs (i.e., Leg₁ vs. Leg₂) were assessed using paired samples *t*-tests. A two-way repeated measures ANOVA (time x condition) was employed to test for differences in the profiles of muscle [PCr], [Pi], [ADP] and pH, aEMG (using 30 s mean values), and RPE (using 120 s mean values). Where the ANOVA revealed a significant main or interaction effect, post-hoc tests were completed using a Bonferroni correction. For calculation of effect size, partial eta squared (η^2) was used for omnibus tests. Cohen's *d* was used to calculate the effect size for paired *t*-tests and post-hoc comparisons. Where sphericity was violated, a greenhouse-geisser correction factor was applied. For all tests, results were considered statistically significant when $P < 0.05$. Data are presented as means \pm SD unless otherwise indicated. All statistical analyses were conducted using IBM SPSS Statistics version 24.

RESULTS

There was no difference in T_{lim} during the Leg₁CON (396 ± 105 s) and Leg₂CON (385 ± 104 s) protocols ($P>0.05$, $d=0.10$, figure 2). Moreover, there were no differences in [PCr], [Pi], [ADP], pH (table 1, figure 3), aEMG amplitude (table 2, figure 5) and RPE (figure 6) between Leg₁CON and Leg₂CON at any time (all $P>0.05$). Compared to Leg₂CON, T_{lim} was reduced by 19% when Leg₂ was preceded by exhaustive exercise in Leg₁ following the consumption of PL (Leg₂CON: 385 ± 104 s vs. Leg₂PL-CONTRA: 311 ± 92 s, $P<0.01$, $d=0.76$, figure 2).

Effect of ACT on single-leg exercise tolerance and contralateral leg fatigue

There was no difference in T_{lim} between the Leg₁CON (396 ± 105 s), Leg₁ACT (402 ± 101 s) and Leg₁PL (390 ± 106 s) conditions ($P>0.05$, $\eta^2=0.07$, figure 2). Both Leg₂PL-CONTRA and Leg₂ACT-CONTRA T_{lim} were significantly lower compared to Leg₂CON ($P<0.05$, $\eta^2=0.71$, figure 2). However, there was no difference in T_{lim} between Leg₂PL-CONTRA and Leg₂ACT-CONTRA (311 ± 92 s vs. 324 ± 85 s, respectively, $d=0.15$, $P>0.05$, figure 2).

Muscle metabolic measurements

The [PCr], [Pi], [ADP] and pH profiles are illustrated in figure 3 for Leg₁PL and Leg₁ACT and in figure 4 for Leg₂CON, Leg₂PL-CONTRA and Leg₂ACT-CONTRA, respectively. There were no significant differences in [PCr], [Pi], [ADP] or pH measured at any time points between Leg₁CON and Leg₂CON ($P>0.05$, table 1, figure 3). Similarly, there were no differences in end-exercise [PCr] (Leg₂CON: 16.0 ± 3.0 , Leg₂PL-CONTRA: 16.1 ± 2.4 , Leg₂ACT-CONTRA: 15.7 ± 2.6 mM, $\eta^2=0.13$), [ADP] (Leg₂CON: 57.8 ± 20.7 , Leg₂PL-CONTRA: 56.4 ± 16.8 , Leg₂ACT-CONTRA: 55.3 ± 17.8 μ M, $\eta^2=0.09$) and pH (Leg₂CON: 6.83 ± 0.15 , Leg₂PL-CONTRA: 6.83 ± 0.20 , Leg₂ACT-CONTRA: 6.80 ± 0.15 , $\eta^2=0.05$) between the Leg₂CON, Leg₂PL-CONTRA and Leg₂ACT-CONTRA conditions ($P>0.05$, table 1, figure 4). However, end-exercise [Pi] was significantly lower in Leg₂PL-CONTRA and Leg₂ACT-CONTRA compared to Leg₂CON (Leg₂CON: 21.8 ± 3.7 , Leg₂PL-CONTRA:

18.8 ± 4.1, Leg₂ACT-CONTRA: 18.7 ± 3.9 mM, $P=0.04$, $\eta^2=0.89$, table 1, figure 4). Baseline [PCr] was significantly higher (36.6 ± 2.1 vs. 33.2 ± 3.2 vs. 33.2 ± 3.1 mM, $P<0.0001$, $\eta^2=3.04$), and [Pi] (Pi: 3.96 ± 0.7 vs. 5.2 ± 1.1 vs. 5.2 ± 1.0 mM, $P<0.01$, $\eta^2=2.13$) and [ADP] (ADP: 5.8 ± 1.2 vs. 11.4 ± 4.3 vs. 11.4 ± 4.5 μM, $P<0.01$, $\eta^2=2.55$, table 1, figure 4) were significantly lower, in Leg₂CON when compared to Leg₂PL-CONTRA and Leg₂ACT-CONTRA, respectively. The rates of change for [Pi] (0.05 ± 0.01 vs. 0.05 ± 0.02 vs. 0.05 ± 0.02 mM/s, $P>0.05$, $\eta^2=0.10$), [PCr] (-0.06 ± 0.02 vs. -0.06 ± 0.04 vs. -0.06 ± 0.03 mmol/s, $P>0.05$, $\eta^2=0.11$), [ADP] (0.15 ± 0.09 vs. 0.17 ± 0.10 vs. 0.15 ± 0.09 μM/s, $P>0.05$, $\eta^2=0.17$) and pH ($P>0.05$, $\eta^2=0.08$) were not different between the Leg₂CON, Leg₂PL-CONTRA and Leg₂ACT-CONTRA conditions, respectively.

Electromyography (n=10)

aEMG amplitude of *m. vastus lateralis* rose significantly from the first minute of exercise to end-exercise in all conditions (figure 5; $P<0.01$, $\eta^2=3.8$). However, there were no differences in aEMG between Leg₁CON, Leg₁PL and Leg₁ACT at T_{lim} (Leg₁CON: 229 ± 54, Leg₁PL: 224 ± 43, Leg₁ACT: 238 ± 51%, $P=0.69$, $\eta^2=0.09$, table 2, figure 5). End-exercise aEMG in Leg₂CON was also similar to Leg₂PL-CONTRA and Leg₂ACT-CONTRA, respectively (Leg₂CON: 234 ± 52, Leg₂PL-CONTRA: 226 ± 58, Leg₂ACT-CONTRA: 242 ± 52%, $P=0.69$, $\eta^2=0.20$, table 2, figure 5). However, absolute aEMG was elevated at the start of Leg₂PL-CONTRA and Leg₂ACT-CONTRA exercise when compared to Leg₂CON (Leg₂CON: 0.04 ± 0.02, Leg₂PL-CONTRA: 0.05 ± 0.02, Leg₁ACT-CONTRA: 0.05 ± 0.02 mV, $P<0.05$, $\eta^2=0.58$, table 2, figure 5).

Ratings of perceived exertion

RPE increased in all trials following the onset of exercise (figure 6). However, there were no differences in RPE between Leg₁CON, Leg₁PL and Leg₁ACT at any time point ($P>0.05$, $\eta^2=0.08$, figure 6). The rate of rise and the end-exercise RPE were also similar during the Leg₂CON trial

compared with the Leg₂PL-CONTRA and Leg₂ACT-CONTRA trials ($P>0.05$, $\eta^2=0.18$). However, at the onset of exercise, RPE was significantly higher in Leg₂PL-CONTRA and Leg₂ACT-CONTRA when compared to Leg₂CON ($P<0.05$, $\eta^2=0.55$, figure 6). Specifically, during the first 2 min of exercise, there was a respective elevation in RPE of 14% and 13% in Leg₂PL-CONTRA and Leg₂ACT-CONTRA, compared to Leg₂CON ($P<0.05$). There were no differences in RPE at any time points between Leg₂PL-CONTRA and Leg₂ACT-CONTRA ($P>0.05$, $\eta^2=0.21$, figure 6).

DISCUSSION

The principal original finding of this study was that, while time to task failure was lower during severe-intensity single-leg knee extensor exercise after the completion of prior fatiguing exercise in the contralateral leg, this effect was not mitigated by acute ACT ingestion. We found no differences in the rates of change or end-exercise values for skeletal muscle activation (via EMG), metabolic perturbation (via ³¹P-MRS) and perception of effort (via RPE) during exercise after prior contralateral leg fatigue following ACT and PL ingestion. Moreover, there were also no differences in time to task failure (i.e., T_{lim}), skeletal muscle activation, metabolic perturbation and RPE during single-leg exercise without the completion of prior fatiguing exercise in the contralateral leg following ACT and PL ingestion. These findings do not support our experimental hypotheses and suggest that 1 g of acute ACT ingestion does not improve time to task failure, skeletal muscle activation, metabolic perturbation or perceived exertion during single-leg severe-intensity knee extensor exercise completed with or without prior fatiguing exercise by the contralateral leg. Collectively, these results contribute to our understanding of fatigue development during exercise, performed with or without prior contralateral leg exercise, and in the presence or absence of ACT ingestion.

298 In the present study, T_{lim} in the Leg₂PL-CONTRA protocol was shorter than the Leg₂CON protocol,
299 indicative of an earlier task failure after completing exhaustive exercise in the contralateral leg
300 compared to no prior fatiguing contralateral leg exercise. This observation is consistent with
301 some (i.e., 3, 14, 22, 29, 33, 41), but not all (i.e., 16, 21, 34, 42, 45), previous studies reporting
302 greater fatigue development after prior contralateral or non-local muscle fatigue. While the
303 neuromuscular bases of contralateral fatigue development have yet to be fully resolved (23),
304 there is evidence to suggest that greater central fatigue makes an important contribution to this
305 phenomenon (3). In the current study, RPE was higher at baseline and over the initial stages
306 of the Leg₂PL-CONTRA test compared to the Leg₂CON test, leading to an earlier attainment of peak
307 RPE and T_{lim} , consistent with previous observations (3) and the notion that afferent feedback
308 may contribute to increased pain and effort sensation (1, 20). Amann and colleagues (3)
309 reported a lower EMG response at task failure and reduced peripheral fatigue development
310 after prior contralateral leg fatigue. Although the EMG amplitude was not different at task
311 failure in the current study between the Leg₂CON and Leg₂PL-CONTRA tests, baseline EMG was
312 elevated in the Leg₂PL-CONTRA condition, presumably due to isometric stabilisation, leading to
313 the earlier attainment of the same peak EMG amplitude. The greater muscle activation in the
314 non-exercising contralateral leg during the baseline ‘resting’ period in the Leg₂PL-CONTRA
315 condition was accompanied by lower muscle [PCr], and higher muscle [Pi] and [ADP],
316 compared to the Leg₂CON condition. Since there were no differences in muscle [PCr] and [ADP]
317 at T_{lim} , and since the rates of change in [PCr] and [ADP] were not different between the Leg₂CON
318 and Leg₂PL-CONTRA tests, the muscle [PCr] nadir and [ADP] peak were attained earlier in the
319 Leg₂PL-CONTRA test. These observations cohere with reports that the end-exercise values of
320 muscle [PCr], [ADP] and pH are consistent when several bouts of exhaustive exercise of
321 differing duration are completed within the severe-intensity domain (7, 44), and when T_{lim} is
322 altered via prior passive heating of the legs (6) or by hyperoxic gas inhalation (44).

Interestingly, however, and despite a higher baseline muscle [Pi] in the Leg_{2PL-CONTRA} condition compared to the Leg_{2CON} condition, muscle [Pi] was lower at the point of task failure in the Leg_{2PL-CONTRA} test. These novel observations suggest that the ergolytic effect of prior contralateral fatigue may be related, at least in part, to a limitation in the attainment of peak intramuscular [Pi].

It is unclear why prior contralateral leg fatigue limited the attainment of peak [Pi] in the Leg_{2PL-CONTRA} condition compared to the Leg_{2CON} condition, whereas the peak [ADP] and the nadir in pH and [PCr] were not different between these conditions. However, our observations of a limited peak perturbation of muscle [Pi], but not pH, [PCr] and [ADP], when group III/IV muscle afferent feedback would be expected to be elevated via prior contralateral fatigue (3), are in accord with studies from another group who observed greater peak perturbation of muscle [Pi], but not pH, [PCr] and [ADP], when group III/IV muscle afferent feedback was abolished via lumbar intrathecal administration of fentanyl (8, 11, 12). Taken together, these complementary observations suggest that intramuscular phosphorous-containing metabolites and substrates may not respond in a uniform manner to manipulations in skeletal muscle group III/IV afferent feedback and that muscle [Pi] might be a more sensitive marker of peripheral fatigue development. However, it should be acknowledged that, since inter-test variability is greater for contracting skeletal muscle [Pi] than for pH, [PCr] and [ADP] (15), further research is required to verify these observations.

Although the completion of prior single-leg fatiguing exercise lowered T_{lim} during subsequent exercise in the contralateral leg in the current study, there were no differences between the Leg_{2ACT-CONTRA} and Leg_{2PL-CONTRA} conditions in T_{lim} , RPE, or muscle activation and phosphorous-containing metabolites and substrates. Similarly, and also in contrast to our

hypothesis, acute ACT ingestion did not alter T_{lim} , RPE, or muscle activation, pH, [PCr], [ADP] or [Pi], during single-leg severe-intensity knee extensor exercise completed without prior fatiguing exercise in the contralateral leg, with these responses being similar between the Leg_{ICON}, Leg_{1PL} and Leg_{1ACT} conditions. These findings conflict with reports that acute ACT consumption can improve exercise performance by increasing work output for the same level of pain and effort sensation (19, 30) and by increasing muscle activation (31, 32).

Experimental Considerations

The lack of an ergogenic effect of ACT administration in the current study might be due to differences in the ACT administration procedure compared to previous studies reporting improved performance and delayed neuromuscular fatigue development (19, 30, 31, 32). In the present study, ACT was ingested 45 min prior to the start of the Leg_{1ACT} test, which immediately transitioned into the Leg_{2ACT-CONTRA} protocol that was the primary focus of the current study. Since peak plasma [ACT] is attained ~60 min post oral ACT ingestion (4, 17), we elected to administer ACT such that peak plasma [ACT] was expected to coincide with the onset of the Leg_{2ACT-CONTRA} protocol rather than the Leg_{1ACT} protocol. This might account for the lack of an ergogenic effect of ACT during the Leg_{1ACT} protocol compared to other studies that administered ACT 60 min prior to the performance trial (19, 30, 31, 32). Therefore, we cannot exclude the possibility that earlier ACT ingestion (18), at the same or a greater dose (19, 30), might have resulted in improved single-leg severe-intensity exercise tolerance. However, it should also be noted that inter-study differences in participant characteristics (i.e., training status, motivation and responsiveness to analgesic medication) may have contributed to the differences in ergogenicity observed following ACT ingestion between the current study and some previous studies (19, 30, 31, 32).

In addition to differences in the ACT dosing procedure, the lack of an ergogenic effect of ACT administration in the current study might be linked to the nature of the fatiguing exercise test administered. Our subjects completed continuous single-leg severe-intensity knee extensor exercise until task failure with no pre-determined end-point (i.e., an ‘open loop’ exercise test). This differs from situations in which ACT ingestion has been reported to be ergogenic, such as completion of a fixed distance (16.1 km) time trial (30), a fixed number of maximal effort repetitions (19, 31), or a fixed duration of maximal effort (32), all of which have a predetermined end point (i.e., a ‘closed loop’ exercise task). Moreover, since exercise-induced pain sensation is positively associated with exercise intensity (5, 13), and since ACT ingestion is suggested to be ergogenic by mitigating pain sensation (19, 30), this might account for the lack of improvement in performance in the longer duration, continuous severe-intensity exercise test we employed compared to the improved exercise performance that has been reported during maximal-intensity exercise (19, 31, 32). With regard to contralateral fatigue development, we cannot exclude the possibility that ACT might have been effective at attenuating the effects of prior single-leg fatigue on T_{lim} during subsequent exercise if a greater degree of contralateral fatigue had been attained. For example, T_{lim} was lowered by 19% in Leg_{2PL-CONTRA} compared to Leg_{2CON} in the current study, whereas Amann et al. (3) reported a much larger (49%) reduction in T_{lim} following contralateral limb fatigue, which would have provided greater scope for an ergogenic effect with ACT ingestion. Moreover, since RPE is higher and T_{lim} is shorter at the same relative exercise intensity when a larger muscle mass is recruited (35), it is possible that ACT ingestion might have improved T_{lim} during exercise after prior fatigue had a larger muscle mass been recruited in either the initial or the subsequent fatiguing exercise task. Further research is required to assess the exercise settings in which ACT administration is more or less likely to be ergogenic.

In conclusion, the completion of prior single-leg fatiguing exercise compromised exercise tolerance during subsequent exercise in the contralateral leg. This ergolytic effect of prior contralateral leg fatigue was accompanied by elevated baseline RPE, muscle activation and [ADP], and lower baseline [PCr], leading to the earlier attainment of peak (RPE, muscle activation and [ADP]) or nadir (muscle [PCr]) values in these variables, and the attainment of a submaximal end-exercise [Pi]. However, acute ACT ingestion was not effective at lowering perceived exertion, increasing muscle activation or intramuscular perturbation or enhancing T_{lim} during single-leg severe-intensity exercise completed with or without prior fatigue in the contralateral leg. These findings do not support an ergogenic effect of analgesia, at least using the ACT administration and exercise testing procedures employed in the current study.

408 **Conflict of interest**

409 The author declares that there is no conflict of interest regarding the publication of this
410 manuscript.

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412 **Acknowledgements**

413 This research was not sponsored by any funding body external to University of Exeter.

414 Jonathan Fulford's salary was supported via an NIHR grant to the University of Exeter
415 (CRF/2016/10027).

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Table 1. Muscle metabolic responses in Leg₁CON, Leg₁PL, Leg₁ACT, Leg₂CON, Leg₂PL-CONTRA and Leg₂ACT-CONTRA conditions.

	Leg ₁ CON	Leg ₁ PL	Leg ₁ ACT	Leg ₂ CON	Leg ₂ PL-CONTRA	Leg ₂ ACT-CONTRA
Muscle metabolic response						
[PCr]						
Baseline PCr (%)	100 ± 0	100 ± 0	100 ± 0	100 ± 0	92 ± 5*	93 ± 4*
PCr at 120 s (%)	70 ± 8	70 ± 8	71 ± 47	71 ± 8	62 ± 9*	63 ± 7*
End-exercise PCr (%)	42 ± 9	41 ± 9	41 ± 8	44 ± 8	45 ± 7	44 ± 8
Rate of change PCr (mmol/s)	-0.06 ± 0.01	-0.06 ± 0.03	-0.06 ± 0.02	-0.05 ± 0.03	-0.06 ± 0.04	-0.06 ± 0.03
[Pi]						
Baseline Pi (%)	100 ± 0	100 ± 0	100 ± 0	100 ± 0	125 ± 24*	126 ± 23*
Pi at 120 s (%)	310 ± 66	313 ± 71	306 ± 62	312 ± 66	316 ± 70	318 ± 64
End-exercise Pi (%)	590 ± 149	590 ± 137	594 ± 156	588 ± 177	459 ± 110*	460 ± 109*
Rate of change Pi (mmol/s)	0.05 ± 0.02	0.05 ± 0.02	0.05 ± 0.02	0.05 ± 0.02	0.05 ± 0.02	0.05 ± 0.02
[ADP]						
Baseline ADP (%)	100 ± 0	100 ± 0	100 ± 0	100 ± 0	200 ± 78*	201 ± 77*
ADP at 120 s (%)	404 ± 161	415 ± 183	400 ± 148	412 ± 170	538 ± 176	516 ± 154*
End-exercise ADP (%)	1028 ± 386	1036 ± 421	1046 ± 409	1024 ± 401	980 ± 316	978 ± 312
Rate of change ADP (μmol/s)	0.15 ± 0.08	0.15 ± 0.09	0.14 ± 0.07	0.15 ± 0.09	0.17 ± 0.10	0.15 ± 0.09
pH						
Baseline pH	7.04 ± 0.01	7.03 ± 0.02	7.05 ± 0.04	7.04 ± 0.03	7.04 ± 0.03	7.05 ± 0.02
pH at 120 s	6.96 ± 0.09	6.94 ± 0.07	6.92 ± 0.08	6.95 ± 0.08	6.93 ± 0.10	6.94 ± 0.08
End-exercise pH	6.77 ± 0.18	6.76 ± 0.15	6.76 ± 0.16	6.83 ± 0.15	6.83 ± 0.20	6.80 ± 0.15

PL, placebo; ACT, acetaminophen; EMG, electromyography; PCr, Phosphocreatine; Pi, Inorganic Phosphate; ADP, Adenosine diphosphate;
 *significantly different from Leg₂CON, $P < 0.05$

Table2. Electromyography (EMG) responses of *m. vastus lateralis* in Leg₁CON, Leg₁PL, Leg₁ACT, Leg₂CON, Leg₂PL-CONTRA and Leg₂ACT-CONTRA conditions.

	Leg ₁ CON	Leg ₁ PL	Leg ₁ ACT	Leg ₂ CON	Leg ₂ PL- CONTRALATERAL	Leg ₂ ACT- CONTRALATERAL
Neuromuscular function						
Baseline EMG _{RMS} amplitude (mV)	0.04 ± 0.01	0.04 ± 0.02	0.04 ± 0.02	0.04 ± 0.02	0.05 ± 0.02*	0.05 ± 0.02*
End-exercise EMG _{RMS} amplitude (%)	229 ± 54	224 ± 43	238 ± 51	234 ± 52	226 ± 58	242 ± 52
EMG _{RMS} amplitude at 120 s (%)	150 ± 27	160 ± 25	166 ± 26	158 ± 29	155 ± 32	158 ± 34

PL, placebo; ACT, acetaminophen; EMG, electromyography; RMS, root mean square; *significantly different from Leg₂CON, *P*<0.05. Data are from 10 subjects.

Legends to figures

Figure 1

Protocol schematic. Visits 1-4 were completed within a replica of the MRI scanner. Subjects completed a single-leg incremental test on the left leg (visit 1, Leg₁) and right leg (visit 2, Leg₂). Subjects then completed a familiarisation session on visits 3 and 4 which comprised a single-leg severe-intensity constant work rate (CWR) test to task failure with Leg₁, Leg₂ and a crossover test where the Leg₁ protocol was repeated and immediately followed by the Leg₂ protocol (interspersed by 10 min of passive recovery). During visits 5 and 6, subjects completed the Leg₁ and Leg₂ protocols, respectively, without oral consumption of any capsules. On visits 7 and 8, subjects commenced the crossover test, 45 mins following the consumption of 1 g maltodextrin (PL) and 45 mins following the consumption of 1 g ACT. Visits 5-8 were completed within the bore of an MRI scanner for assessment of intramuscular phosphorous substrates and metabolites and then replicated within a replica of the MRI scanner (visits 9-12) to assess muscle electromyography (EMG) and ratings of perceived exertion (RPE). The dashed vertical lines represent the limit of tolerance (i.e., T_{lim}) for each trial and/or leg, respectively.

Figure 2

Exercise tolerance (time to task failure, s) in Leg₁CON, Leg₂CON, Leg₁PL, Leg₂PL-CONTRA, Leg₁ACT and Leg₂ACT-CONTRA conditions. Data are presented as mean ± SD *significantly different from Leg₁CON, Leg₂CON; Leg₁PL and Leg₁ACT ($P<0.05$).

Figure 3

Intramuscular phosphocreatine concentration ([PCr]; panel A), inorganic phosphate concentration ([Pi]; panel B), adenosine diphosphate ([ADP]; panel C) and pH (panel D) during

severe-intensity, single-leg knee-extensor exercise in the left leg following PL ingestion (Leg₁PL, filled circles) and ACT (Leg₁ACT, clear circles) ingestion. Data are expressed as group mean \pm SE.

Figure 4

Intramuscular phosphocreatine concentration ([PCr]; panel A), inorganic phosphate concentration ([Pi]; panel B), adenosine diphosphate ([ADP]; panel C) and pH (panel D) during severe-intensity, single-leg knee-extensor exercise in the right control leg (Leg₂CON, open triangles) and in the right leg following prior exhaustive exercise in the left leg after PL ingestion (Leg₂PL-CONTRA, filled circles) and ACT (Leg₂ACT-CONTRA, clear circles) ingestion. Data are expressed as group mean \pm SE. *T_{lim} significantly different from Leg₂PL-CONTRA and Leg₂ACT-CONTRA ($P < 0.05$); #significantly different from Leg₂PL-CONTRA and Leg₂ACT-CONTRA ($P < 0.05$).

Figure 5

Surface electromyography (EMG) of the *m.vastus lateralis* muscle during severe-intensity, single-leg knee-extensor exercise in Leg₁PL (filled circles) and Leg₁ACT (clear circles) (panel A), and in the right control leg (Leg₂CON, open triangles), and in Leg₂ following prior exhaustive exercise in Leg₁ after PL (Leg₂PL-CONTRA, filled circles) and ACT (Leg₂ACT-CONTRA, clear circles) ingestion (panel B). Mean values for average rectified EMG (aEMG) during each muscle contraction were calculated and averaged over each 30-s period. Data are expressed as group mean \pm SE relative to the first 30 s of each trial. *T_{lim} significantly different from Leg₂PL-CONTRA and Leg₂ACT-CONTRA ($P < 0.05$).

Figure 6

647 Ratings of perceived exertion (RPE) during severe-intensity, single-leg knee-extensor exercise
648 of the left leg in Leg₁PL (filled circles) and Leg₁ACT (clear circles) (panel A), in the right control
649 leg (Leg₂CON, open triangles), and in the right leg following prior exhaustive exercise in the left
650 leg after PL ingestion (Leg₂PL-CONTRA, filled circles) and ACT (Leg₂ACT-CONTRA, clear circles)
651 ingestion (panel B). Data are expressed as group mean \pm SE. *T_{lim} significantly different from
652 Leg₂PL-CONTRA and Leg₂ACT-CONTRA ($P < 0.05$); #RPE significantly different from Leg₂CON
653 ($P < 0.05$).